

**RESEARCH ON THE DEVELOPMENT OF PORTABLE ALCOHOL
BIOSENSORS AND PHARMACOTHERAPY**

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ABSTRACT :

The importance of microfluidics- and micro electro mechanical systems-based biosensors has received widespread recognition, and numerous publications have examined its potential uses in forensics, personalised medicine, global health, clinical diagnostics, and other fields. There is an increasing need to use point-of-care testing to remotely monitor patients' health conditions as a result of rising healthcare expenses. There is a growing need for biosensors to identify biological warfare agents, and research is concentrating on how to make compact, portable devices that would enable on-site, quick, and accurate detection. Due to developing infections that are resistant to pesticides, increased human mobility, and rules restricting the use of hazardous chemicals to stop the spread of illness, there has been an increase in the demand for quick and accurate on-site diagnosis of plant diseases over the past ten years. Biosensors' portability for on- site diagnosis is constrained by a number of factors, such as sample preparation methods, fluid handling methods, the short shelf life of biological reagents, device packaging, integrating electronics for data collection and analysis, and the need for external accessories and power. The application of droplet-based microfluidics, paper-based microfluidic devices, wireless networking capabilities for data transfer, and other microfluidic, electronic, and biological design methodologies are just a few that are currently being investigated.

KEYWORDS : Road accident; Alcohol; Biosensor; Biomarkes; scope

INTRODUCTION :

Road accidents are one of the main causes of death worldwide, killing around 1.3 million of people per year, particularly children and young adults Alcohol abuse is a serious public health issue. According to the Centres for Disease Control (2013), alcohol is a factor in 88,000 deaths per year in the US, and its yearly economic costs are estimated at \$249 billion (Sacks, Gonzales, Bouchery, Tomedi, & Brewer, 2015). Many efforts have been devoted to creating treatments that can assist people in consuming less alcohol in response to this important cause of disease. A crucial part of treating alcohol consumption disorder (AUD) is pharmacotherapies. The Food and Drug Administration (FDA) has currently approved three drugs to treat AUD: naltrexone (oral and injectable), disulfiram, and acamprosate. Despite the fact that these drugs work for some patients, many people who take them eventually resume heavy drinking (Jonas et al., 2014). New pharmacotherapies for AUD are a top priority for the National Institute on Alcohol Abuse and Alcoholism (NIAAA) (Litten, Falk, Ryan, & Fertig, 2016). Finding effective novel drugs will lead to better treatment outcomes, especially for patient populations for whom currently available drugs are less successful (Garbutt et al., 2014). The development of AUD

medications has numerous challenges, including low treatment effect sizes (Jonas et al., 2014), significant participant attrition (Hallgren & Witkiewitz, 2013), and uncertainty regarding the best laboratory screening models and clinical objectives. When promising pharmacotherapies are tried on humans, these hurdles are a factor in the lacklustre performance of those treatments (Litten, Wilford, Falk, Ryan, & Fertig, 2016). In order to improve the effectiveness and predictive validity of this research, NIAAA has acknowledged the problems that impede the development of new medications. Finding translational paradigms to evaluate potential treatments for early efficacy and safety in humans is one of the plan's two key components, along with improving the methodological quality of pivotal phase 3 clinical trials.

ALCOHOL BIOMARKERS

Forensic analysis, therapeutic practise, and the use of alcohol in inappropriate settings are all areas of research that place a high value on alcohol detection and quantification. Typically, ethanol is absorbed by simple diffusion through the stomach mucosa (20%) and little intestine (80%). Alcoholic beverages contain the kind of alcohol known as ethanol. 2022, 12, 252, 3 of 30 Biosensors In urine, sweat, saliva, and faeces, 2% to 10% of all ethanol consumed is removed. breathed out. Three distinct pathways Alcohol Dehydrogenase (ADH), System Microsomal Oxidation of Ethanol (SOME), and catalase signalling pathway oxidize about 90% of it in the liver. Maurice Nicloux and Widmark created the first techniques for measuring the amount of ethanol in blood in 1906 and 1920-1930, respectively. In these techniques, volatile chemicals like ethanol were eliminated from the blood via diffusion. utilising glass flasks in particular, followed by oxidation with chromic acid and volumetric analysis with iodometric titration. For many years after its invention, Widmark's approach was utilised throughout the world to evaluate criminals and drivers. The utilisation of various biological matrices has become even more feasible and accessible with the advent of new techniques for analyte extraction. The most common ones are sweat, exhaled air, hair, saliva, and vitreous humour in addition to blood and urine. Any substance or element whose concentration is present in a certain biological fluid and can be utilised as a marker for a specific disease or physical condition is referred to as a biomarker. Alcohol indicators are widely used in medicine and public security. They can be used to monitor the development of disorders linked to this health issue or any hereditary predisposition towards alcohol misuse in addition to providing an objective parameter of alcohol consumption to aid in the diagnosis of alcohol abuse. These are the primary alcohol biomarkers:

ETHANOL: most reliable and well-researched validating biomarker. Due to its brief half-life in the body, ethanol can only be used recently. All of the previously described biological matrices contain this biomarker.

EtG (ethylglucuronide) : the ethanol's primary metabolite. Despite making up just around 0.1% of the total amount of ethanol disposed of, EtG has a long window of detection, allowing it to be found in blood and urine up to 36 hours and 5 days after binge drinking, respectively. False-positive results could be caused by accidental exposure to goods containing ethanol, even yeast and sugar. while false-negative results for some urinary tract infections are possible Other biological matrices like sweat and hair can be detected using this biomarker with good results.

EtS (ethylsulfate) : a direct metabolite of ethanol with relapse biomarker potential comparable to EtG. The combination of these two ethanol-specific metabolic products can more accurately identify recent alcohol usage.

FAEEs (fatty acid ethyl esters) : The majority of these glands are found in the face and hair. However, it can occur anywhere on the body except the hands, feet, and palms. These alcohol-related byproducts have been documented. to last up to almost 100 hours in the blood of heavy drinkers. Blood and hair are the biological matrices most frequently utilised to detect this biomarker.

CDT (carbohydrate-deficient transferrin) : powerful biomarker for long-term ethanol consumption. Asialo-, monosialo-, and disialotransferrin, which contain zero, one, and two sialic residues, respectively, are examples of minor forms of transferrin with lower levels of glycosylation that are referred to as CDT. In healthy individuals, many variations of this glycoprotein are present. However, research indicates that alcohol use raises the levels of this chemical concentrations. The CDT has sensitivity and specificity ranges of 60-70 and 80-95%, respectively. Other medical issues unrelated to alcohol usage, like anorexia nervosa and pregnancy, may have an impact on CDT levels. Furthermore, it has been demonstrated that it is challenging and imprecise to assess CDT. Blood and urine are the most often utilised biological matrices.

?-HEX (?-hexosaminidase) : is a lysosomal hydrolase that functions in the liver's ganglioside and glucose metabolism. Lysosomes are broken after consuming a lot of alcohol, which causes the release of the enzyme into the bloodstream.

In serum, -HEX has a half-life Biosensors 2022, 12, 252 4 of 30 of about 6.5 days. According to reports, the sensitivity of serum and urine -HEX activity is 69-94 and 81-85%, respectively. The specificity of urine and serum -HEX activity is 84-96% and 91-98%, respectively. However, those with hypertension, diabetes, and diab

The most precise biomarkers for identifying alcohol intake are, in essence, ethanol and EtG. The most precise way to assess someone's alcohol level is using an ethanol test. However, after the first 6-12 hours, this analyte cannot be consistently found in bodily fluids. Since EtG is an ethanol direct metabolite that may detect alcohol for a few days, there has been an increase in interest in the study of EtG as an alcohol biomarker.

Although studies have discovered that EtG has greater maximum concentrations than EtS and have concluded that EtS assay is more labor-intensive and offers minimal advantage over EtG despite having similar potential to EtS as a biomarker of relapse,

Heavy drinkers' FAEEs can remain increased for up to 99 hours, but they cannot be seen in the hands' and feet's palms. ethanol's indirect metabolite CDT is a long-term indicator of high alcohol consumption. alcoholic beverage use. However, those suspected of having glycosylation disorders, anorexia nervosa, or pregnant ladies cannot be checked. Testing for -HEX is not advised since it may yield false-positive results in some situations. drinking biomarkers already offer a significant amount of critical information that can be used to help with drinking disorder prevention and treatment. However, more study is required in order to identify biomarkers with greater sensitivity and, in turn, overcome the limits of the already employed biomarkers for alcohol intake.



BIOSENSOR : Engineering, physics, chemistry, and biology transdisciplinary research are needed to build a biosensor. The target biomarker, particularly in terms of its molecular characteristics and concentration range, often influences the choice of materials and methodologies.

A biosensor is made up of the bioreceptor, the transducer, and the processing system [58,62]. Examples of bioreceptors include enzymes, antibodies, aptamers, molecular imprinted polymers (MIPs), and others. The target analyte (biomarker) interacts with the bioreceptor to generate an effect that may be recognised and quantified by the transducer, which converts it into a signal proportionate to the target analyte's presence in a sample. The processing system can view, amplify, and store this signal.

HISTORY OF BIOSENSOR :

Leland C. Clark performed the initial test that established the biosensor as a distinct technology. Platinum (Pt) electrodes were employed by Clark to detect oxygen in his experiment. By trapping the enzyme glucose oxidase (GOD) against the electrodes with a piece of dialysis membrane, he was able to bring it extremely near to the surface of platinum. The enzyme activity changed depending on how much oxygen was present. When glucose and glucose oxidase (GOD) interact, gluconic acid is produced along with two electrons and two protons, decreasing GOD. additional GOD is made available for additional glucose to react with as a result of the reaction between the reduced GOD, the electrons, protons, and the surrounding oxygen. This reaction results in hydrogen peroxide and oxidised GOD (the original form).

BIOSENSORS CAN BE CLASSIFIED ACCORDING TO THE TRANSDUCER USED :

Optical biosensors : The primary goal of analytical instruments with a biorecognition component built into an optical transducer system is to generate a signal that is proportionate to the concentration of the substance being measured (the target analyte).

Thermal biosensors : To determine the concentration of the analyte, measure the heat produced by exothermic enzyme catalytic processes. High-sensitivity thermistors are typically used to measure temperature changes. These biosensors are difficult to use.

Piezoelectric biosensors : this are based on the piezoelectric quality that anisotropic crystals, like quartz, have. This biosensor responds to an alternating voltage by oscillating with a crystal at a frequency related to the mass and elastic properties of crystals

Electrochemical biosensors : Pertaining to producing an electrical signal that is correlated with the intended analyte concentration in the sample. Ions or electrons that impact electrical behaviour, such as current or electrical discharge, are produced or consumed during chemical reactions between an immobilised bioreceptor and the target analyte. Potential.

The most popular forms of biosensors are electrochemical ones, which have been proved to be the most successful in biofluid analysis due to their great adaptability, low cost, ease of production, and high sensitivity. and selectivity, quick detection, ease of use, and adaptability to wearable, portable, and miniaturised devices. Electrochemical biosensors are categorised based on the electrochemical method used to quantify the residuum, which is how the analyte is quantified.



ELECTROCHEMICAL TECHNIQUES:-

Analysing the loss (oxidation) or gain (reduction) of electrons that a given material experiences during an electrical stimulus requires the application of electrochemical techniques. The concentration, kinetics, and other data are provided by these oxidation- reduction (redox) reactions. reaction processes and additional species-specific behaviours in solutions [68]. Nevertheless, a variety of electrical parameters, including voltage, current, charge, and time, can be obtained from electrochemical measurements, allowing for the evaluation of a biosensor's performance. As previously mentioned, electrochemical biosensors can be divided into groups based on the traits of the signal produced during transduction. Biosensors can therefore be classed as potentiometric, amperometric, or impedimetric depending on the type of signal, which can be potential difference, current intensity, or changes in impedance or conductance, respectively.

Potentiometric : The potential difference between the working electrode and the reference electrode is measured using potentiometric biosensors. When an antigen-antibody interaction, for instance, takes place, this potential difference is created and measured under practically none at the moment

Amperometric : When a constant (in the case of chronoamperometry measurements) or variable (in the case of voltammetry measurements) of potential is applied to the working electrode, amperometric biosensors measure the current produced due to electrochemical oxidation or reduction of electroactive species at the working electrode. regarding the reference electrode. The measured current is proportional to the concentration of the target analyte and represents the rate of transferred electrons over time.

Impedimetric biosensors : Impedimetric biosensors gauge the electrical resistance that is created at the electrode contact in response to a tiny sinusoidal perturbation signal. The sensor electrode must be exposed to low amplitude AC voltage, and then, using an impedance analyzer, the current response is determined as a function of frequency.

MOBILE BIOSENSORS FOR ALCOHOL CONSUMPTION DETECTION

As alcohol is taken, metabolised, and expelled, numerous quantifiable biosignals are generated during or after drinking. These signals can be picked up by biosensors. Although drinking produces a variety of bio signals that can be picked up by the right sensors, transdermal alcohol detection has received the majority of current attention in research on alcohol biosensor technology. About 1% of the alcohol that is consumed is eliminated in perspiration, and the amount of alcohol in sweat has a roughly linear relationship with blood alcohol levels. Similar to fuel cell breathalysers, transdermal alcohol sensors (TAS) can continually check the alcohol concentration of perspiration. Alcohol is oxidised on a sensor that is placed against the skin; the oxidation current is then measured and used as a gauge for the amount of alcohol present. Continuous samples can be taken at predetermined intervals (like every 10 seconds).

Researchers can presently choose between two TAS models. Both the Wrist Transdermal Alcohol Sensor and the Secure Continuous Remote Alcohol Monitor (SCRAM; Alcohol Monitoring Systems) are TASs that are worn on the ankle. Data are wirelessly sent using a specialised modem or over a connected connection to a user's PC after being temporarily stored onboard the device. Both devices have sensors that can detect when the gadget is removed, including temperature and skin

resistance/conductance sensors. The SCRAM has a tamper-proof band to make it difficult to take the gadget out. Both tools have been successfully employed in lab-based research. The SCRAM has been used successfully in forensic settings to monitor DUI offenders as well as clinical trials of contingency management for heavy drinking.

The transdermal alcohol concentration (TAC) of the wearer is measured by both the SCRAM and the WrisTAS. TAC measurements are continuously taken and either saved on the device itself or instantly relayed to another linked device for storage. A timestamp, TAC, skin temperature, and, in models with the required sensors, skin conductance and resistance, are all recorded along with the measurements in a database. TAS can collect a lot of readings every day (like 86,000+), producing a lot of data because readings are done continually. The study procedure calls for the combination and transformation of these unprocessed observations. For instance, the number of days without drinking or the distinction between episodes of moderate and excessive drinking may be of interest to researchers. Charting TAC during a drinking event can be used to estimate BAC and infer pharmacokinetic factors, such as peak BAC and rate of BAC rise.

Currently, the "next generation" of TAS is being created. These gadgets are similar to other "smart" health monitoring "devices" that are offered for sale (such as smartwatches and wrist-worn activity trackers). One such device is the wrist-worn TAS BACTrack Skyn (BACTrack, Inc.), which is still under development but almost ready. The first next-generation TAS to be made available to the general public will probably be the BACTrack Skyn. Since we have expertise with the BACTrack Skyn (other businesses are also creating new TAS), we use it as an example when describing the new TAS. Compared to SCRAM and WrisTAS, these new devices will be more discrete and smaller. The Skyn's settings can now be changed to suit the user's preferences and are more customizable (for example, the user can specify how frequently readings are taken). They will also have enhanced wireless connectivity and be able to quickly transfer data using Bluetooth to other devices (such as smartphones), enabling the transmission and real-time presentation of TAS data. While such improvements might be added in later versions, we are not aware of any new TAS that are being built with tamper deterrents. Our study team has had early access to prototype units from BACTrack, Inc., and we have successfully used the tools for lab-based testing. Participants in our initial testing were able to wear and use the gadget with little difficulty and social or bodily discomfort. Such next-generation devices will probably be more suitable for long-term alcohol use monitoring for clinical and research populations.



Figure 1: A BACtrack Skyn prototype connected to a smartphone. The prototype shown above is not the final manufacturing item. The programme shown is an alpha version intended for demonstration purposes.

MOBILE BIOSENSORS FOR IMPROVING AUD PHARMACOTHERAPY RESEARCH

A semi-sequential series of studies that are designed to rigorously assess the effects of pharmaceuticals on health and alcohol use behaviour make up the pipeline for the development of AUD medications. The pipeline for developing new pharmaceuticals aims to find safe and efficient pharmacotherapies and bring these medicines swiftly and cheaply towards widespread clinical use. Despite the fact that preclinical research is crucial to this process, this article will concentrate on human research. The AUD medication human research pipeline is shown in Figure 2. The development process for AUD medication will be reviewed in this part, along with the integration of mobile biosensors into common paradigms.

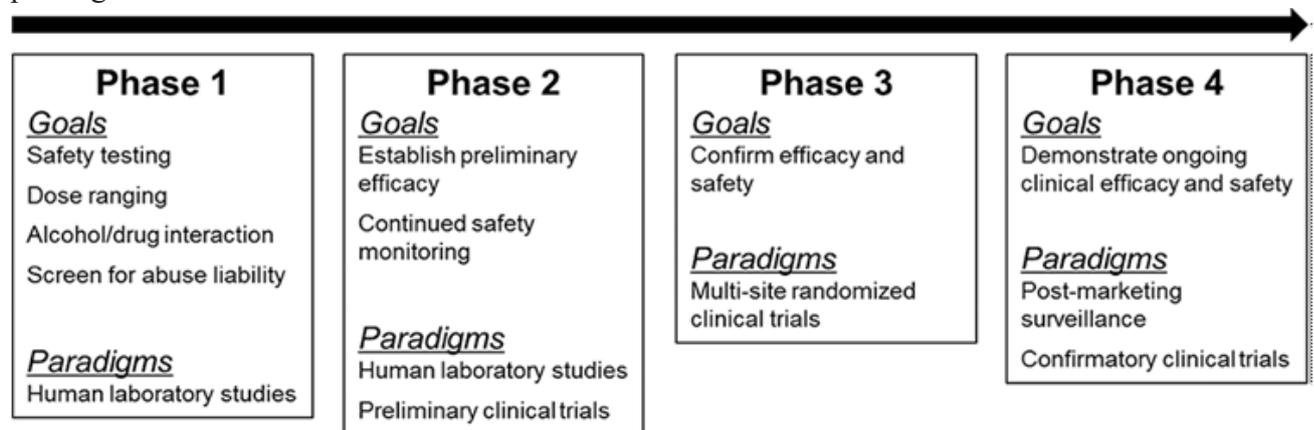


Figure 2. Each stage of human testing in the AUD drug development pipeline has its own set of goals and paradigms.

Phase 1: Testing for Safety and Tolerability

The primary goal of phase 1 human research is to determine if new drugs are safe and acceptable in humans and to define optimal dose methods. Participants in Phase 1 trials are usually healthy volunteers, and the research takes place in a controlled laboratory under medical supervision. With a few exceptions, participants will not be given alcohol while taking a candidate drug during phase 1 testing. Even when alcohol is administered (as in alcohol/drug interaction screening), volunteers are closely monitored for their own safety. Direct assessment procedures (e.g., blood draw, breath sampling) can provide a more accurate estimate of BAC than mobile biosensors for monitoring alcohol pharmacokinetic data. For these reasons, mobile biosensors are unlikely to play a significant role in phase 1 testing.

Phase 2: Human Laboratory Studies and Clinical Trials to Proof-of-Concept

Phase 2 laboratory studies are frequently the first to assess a drug's potential for treating a human condition. Studies conducted in laboratories are ideal for this use. The laboratory setting gives researchers complete control over the testing environment, minimising the impact of obtrusive variables. Since results are directly witnessed, measurement error is kept to a minimum. As a result, the effects of medications on the outcomes of alcohol use are quite sensitive in these research. The creation of procedures that increase this research's predictive validity is currently of great interest.

Laboratory research on humans assess how drugs affect behavioural simulations of real-world alcohol consumption consequences. Table (1) provides a list of common paradigms and their respective drug targets. These processes are modelled using a variety of paradigms, as can be seen in the table. Directly measuring alcohol consumption while engaging in a self-paced drinking assignment is the most direct approach. Utilising paradigms for fixed-dose alcohol administration is another method for assessing alcohol reactivity. The main outcome variables are the amount of ad libitum drinking and the responsiveness to alcohol. Studies on humans in laboratories can also reveal the behavioural mechanisms through which drugs lower alcohol use. For instance, specific analyses of the subjective effects of alcohol during fixed-dose alcohol administration can reveal whether some drugs lessen the energising, reinforcing effects of alcohol. Clearly, human laboratory paradigms provide significant contributions to AUD medication testing; nonetheless, these methods have well-known drawbacks. The organisation of laboratory sessions including the administration of alcohol requires considerable financial and human resources from an efficiency perspective. Most laboratory screening investigations only watch people during the first or second drinking episodes, giving an insufficient picture of the underlying feature. The fact that drinking in the lab is a poor substitute for alcohol usage that occurs in nature is another significant limitation of this study. The regulated context in which human laboratory experiments are conducted may restrict the external validity of the study.

Phase 2:- clinical trials to proof-of-concept

Clinical trial testing follows a human laboratory study that confirms a drug's efficacy as the next step in the pipeline. Phase 2 proof-of-concept clinical studies are crucial since they are frequently the first to assess a drug's effectiveness when it is used in a setting similar to a clinic. By converting findings from the laboratory to clinical outcomes, these trials play the role of a bridge between large-scale pivotal Phase 3 testing and human laboratory investigations. Patients are randomly assigned to receive active medication or a placebo, and their drinking is monitored during the course of therapy, according to the gold-standard design for drug testing (randomised clinical trials). The primary objective used to gauge treatment efficacy is predetermined by the investigators. Typically, primary outcomes are based on patient-reported data.

Mobile biosensors are being tested in proof-of-concept Phase 2 clinical trials

In proof of concept clinical trials, mobile biosensors have the potential to replace self-reported drinking or possibly serve as a replacement. In treatment trials for other substances of abuse, biological verification of abstinence-typically determined through urine toxicology-is normal procedure. Platforms for mobile biosensors will offer an unbiased, scientifically verifiable record of abstinence.

Researchers will be able to gather a wide range of secondary clinical outcomes using the biosensor system. There are numerous secondary endpoints based on biosensors that could be assessed, as shown in Table 3. Many of the triggered assessments discussed in the preceding section could also be employed during these clinical trials if drinking is found because data is continuously collected and given.

The ecological validity of these evaluations can be increased by measuring secondary self-report outcomes like desire when patients are away from the clinic. Data gathering during crucial events, such as the first relapse after a period of sobriety, will be made easier by this ongoing monitoring. Real-time

data gathered during relapse episodes will shed light on the contextual factors that contribute to relapse, which will provide mechanistic information on the drug under test and, perhaps more crucially, shed light on why certain people struggle to maintain sobriety.

Additionally, a smartphone-connected biosensor platform can be used to maintain constant communication with clinical study participants. During a treatment phase, participants in clinical trials typically go to weekly or biweekly clinic sessions. Participants often give biopsies, report adverse events, report primary outcomes (such as past-week drinking) and secondary outcomes (such as cravings), and receive their weekly supply of medicine during these clinic sessions. A common component of clinic appointments is behavioural treatment. When biosensors are used in clinical trials, many of these tasks become unnecessary because outcome variables, such as alcohol consumption, self-reported outcomes, and adverse events, can be tracked passively or by prompting from mobile devices. The smartphone platform can be used to deliver automated behavioural treatments. In fact, recent efforts to computerise the delivery of behavioural therapies, particularly those for substance use disorders, have made tremendous progress. Less clinic visits will be required if communication with patients is predominantly done through a biosensor-linked platform with a smartphone user interface. This change will lessen the workload for both the staff and the patients and could improve retention. Smartphones can be used to send medicine reminders, which is another possible use of constant remote communication with patients. Medication use can be instantly reported and verified. The low rates of drug compliance among participants in AUD pharmacotherapy clinical trials may be improved by this system. Despite the significant advantages of mobile biosensors in improving the detection of alcohol use during clinical trials, further study is required to demonstrate the usefulness and acceptability of these devices. Although early research has shown that heavy drinkers can use mobile biosensors over the long term in treatment studies, it will be crucial to show that patients are able and willing to wear newer biosensors (like the BACtrack Skyn) that can be removed and require periodic charging. Finding the optimal definition of treatment response using data from mobile biosensors will be another top objective. Endpoints based on predicted BAC cutoffs may be more sensitive markers of therapy response than the quantity of drinks. It will be crucial for researchers to carefully pick the tools and detection standards that best meet the requirements of their methodology. Biosensors with high sensitivity to detect low-level drinking episodes, for example, would be ideal for clinical trials. When detecting heavy drinking is the primary goal, biosensors with more conservative detection parameters may be preferable.

Phase 3: Special Considerations for Pivotal Clinical Trials

Phase 3 clinical trials follow the same procedures as Phase 2 proof-of-concept studies, but they are more expensive and larger. Since Phase 3 clinical trials use biosensors, many of the advantages of utilising them in proof of concept studies also apply to them. However, there are certain other considerations that are unique to the use of biosensors in Phase 3 pivotal trials. For a pharmaceutical to receive regulatory approval, clinical trials must be conducted, and the design and reporting of results must adhere to a set of rules. The active treatment phase of pivotal trials lasts for up to six months, during which participants continue to take their medications and see their doctors on a regular basis. Following the active treatment phase, follow-up evaluations are done to see how long the benefits of the treatment have lasted.

Regarding appropriate primary endpoints, the FDA and other regulatory organisations provide clear recommendations. At the moment, acceptable endpoints are determined by self-reports of alcohol consumption, which are typically gathered via a daily drinking diary or timeline follow-back. The number of participants without heavy drinking days or the percentage of participants who successfully abstain from alcohol are the acceptable endpoints according to the current criteria in the United States. These endpoints were chosen based on secondary analysis of extensive clinical trials that investigated which outcomes were most responsive to decreases in drinking-related effects. These decisions were made based on assessments of self-reported drinking patterns. Additional study will be needed to choose an ideal endpoint with highest sensitivity to treatment effects and good predictive validity when mobile biosensors are used in crucial clinical studies.

By automatically sending trial results to a centralised server location, mobile biosensor platforms could simplify multisite clinical studies. Efficiency can be improved by centralising data storage and easing the burden of data management. Additionally, biosensor-based assessment's remote nature and reduced participant load may make it easier to quickly find a more representative sample of participants.

Phase 4: Postmarketing monitoring and dissemination

Phase 4 testing includes systematic evaluation of the use and efficacy of approved drugs in real-world settings, as well as confirmatory clinical trials that take place after a medication is approved to treat AUD. Given the low rates of treatment utilisation among people with AUD, less attention has been placed on Phase 4 research in the AUD treatment development sector. However, future research in this area could have a significant impact on public health. Mobile alcohol biosensors could have a role in routine clinical care in the future, particularly for persons being treated for alcohol-related health problems. Because the data acquired by these biosensors is digitised, treatment outcomes may be easily aggregated and analysed to assess drug efficacy in clinical settings. Mobile alcohol biosensors, as a consumer product, have the potential to raise awareness of dangerous alcohol intake and allow communication between patients and healthcare providers in the same way that other home health monitoring devices do.

OUTLOOK AND FUTURE SCOPE :

The ability of the conventional industry of textiles to innovate will determine how quickly it can expand. This industry has to be reimagined if it is to reach its full potential and maintain its competitiveness. The secret is to encourage innovation to offer value while always anticipating the demands and trends of the market. Globally, there is an exponential increase in demand for the production of intelligent fabrics and smart materials. Therefore, this study looked at the most advanced sweat-based biosensors for alcohol detection. and aims to inspire the reader to conduct further research by outlining a number of innovative hypotheses that aim to advance the textile industry by creating new textile-based biosensors that enhance human life, specifically alcohol biosensors to lessen drunk driving incidents, traffic accidents, and the ensuing premature death or disability of drivers, passengers, and pedestrians. One of the greatest scientific endeavours in recent years has been the creation of biosensors as non-invasive tools for simple monitoring and quick assessment of a person's health state. The study on biosensors that can identify ethanol in sweat as well as viruses and illnesses including diabetes, heart failure, circulatory problems,

metabolic and respiratory diseases, among others, has been covered in this review paper. However, because of the immaturity of this market sector, it is vital to experiment with novel approaches and make items that are cutting-edge and useful in order to capture consumers' attention. However, further study is needed to ensure the long-term dependability and repeatability of biosensors. The type of bioreceptor utilised, or the substance that gives the biosensor its selectivity, frequently compromises the durability of a biosensor. Biosensors often have limited stability and durability due to the integration of bioreceptors like enzymes, antibodies, and aptamers since they end up being less resistant to harsh conditions like high temperatures, high pressure, and pH fluctuations. Thus, a substitute method known as "molecular printing" has just lately been developed to address this issue and enable the artificial fabrication of these structures.

REFERENCES :

1. WHO Kicks off a Decade of Action for Road Safety. 2021. Available online: <https://www.who.int/news/item/28-10-2021-who-kicks-off-a-decade-of-action-for-road-safety> (accessed on 1 April 2022).
2. Simões, M.T.B.d. Fatores de Risco Auto Reportados Associados aos Acidentes Rodoviários: Um Estudo Sobre os Condutores Portugueses de Veículos Ligeiros. 2014. Available online: <https://run.unl.pt/handle/10362/14807> (accessed on 19 December 2021).
3. WHO. 2018. Available online: <https://www.who.int/news-room/fact-sheets/detail/alcohol> (accessed on 8 March 2022).
4. Azevedo, A.M.; Miguel, D.; Prazeres, F.; Cabral, J.M.S.; Fonseca, L.P. Ethanol biosensors based on alcohol oxidase. *Biosens. Bioelectron.* 2005, 21, 235-247. [Google Scholar] [CrossRef] [PubMed]
5. Fekete, A. Identification of Bacterial N-Acylhomoserine Lactones (AHLs) with a Combination of Ultra-Performance Liquid Chromatography (UPLC), Ultra-High-Resolution Mass Spectrometry, and In-Situ Biosensors; Springer: Berlin/Heidelberg, Germany, 2006. [Google Scholar] [CrossRef]
6. Jenkins, A.J. *Drug Testing in Alternate Biological Specimens*; Humana Press: Totowa, NJ, USA, 2008. [Google Scholar] [CrossRef]
7. Campbell, A.S.; Kim, J.; Wang, J. Wearable electrochemical alcohol biosensors. *Curr. Opin. Electrochem.* 2018, 10, 126-135. [Google Scholar] [CrossRef] [PubMed]
8. RAli, S.S.; Wilson, M.P.; Castillo, E.M.; Witucki, P.; Simmons, T.T.; Vilke, G.M. Common Hand Sanitizer May Distort Readings of Breathalyzer Tests in the Absence of Acute Intoxication. *Acad. Emerg. Med.* 2013, 20, 212-215. [Google Scholar] [CrossRef]
9. Caravati, E.M.; Anderson, K.T. Breath Alcohol Analyzer Mistakes Methanol Poisoning for Alcohol Intoxication. *Ann. Emerg. Med.* 2010, 55, 198-200. [Google Scholar] [CrossRef] [PubMed]
10. Raza, T.; Qu, L.; Khokhar, W.A.; Andrews, B.; Ali, A.; Tian, M. Progress of Wearable and Flexible Electrochemical Biosensors with the Aid of Conductive Nanomaterials. *Front. Bioeng. Biotechnol.* 2021, 9, 761020. [Google Scholar] [CrossRef] [PubMed]
11. Wang, Y.; Xu, H.; Zhang, J.; Li, G. Electrochemical Sensors for Clinic Analysis. *Sensors* 2008, 8, 2043-2081. [Google Scholar] [CrossRef] [Green Version]
12. Li, Q.; Wu, J.-T.; Liu, Y.; Qi, X.-M.; Jin, H.-G.; Yang, C.; Liu, J.; Li, G.-L.; He, Q.-G. Recent advances in black phosphorus-based electrochemical sensors: A review. *Anal. Chim. Acta* 2021, 1170, 338480. [Google Scholar] [CrossRef]
13. Buono, M.J. Sweat Ethanol Concentrations are Highly Correlated with Co-Existing Blood Values in Humans. *Exp. Physiol.* 1999, 84, 401-404. [Google Scholar] [CrossRef]
14. Kamei, T.; Tsuda, T.; Mibu, Y.; Kitagawa, S.; Wada, H.; Naitoh, K.; Nakashima, K. Novel instrumentation for determination of ethanol concentrations in human perspiration by gas chromatography and a good interrelationship between ethanol concentrations in sweat and blood. *Anal. Chim. Acta* 1998, 365, 259-266. [Google Scholar] [CrossRef]
15. Wang, J. *Analytical Electrochemistry*, 3rd ed.; Wiley-VCH: New York, NY, USA, 2006; Available online: <https://www.wiley.com/en-us/Analytical+Electrochemistry%2C+3rd+Edition-p-9780471678793> (accessed on 5 April 2022).